Molecular Imprinted Graphene Oxide Nanocomposite for Optical Sensing of Nicotine in Human Blood Plasma

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Summary: Among all psychotropic alkaloids, nicotine is more addictive, carcinogenic and capable of causing many health problems. This work is based on the development of highly robust, cheap, reliable, selective and sensitive nicotine imprinted graphene oxide nanocomposite (ImpGO nanocomposite) based optical sensor for determination of nicotine in human plasma. The ImpGO nanocomposite has been thoroughly characterized using different techniques i.e. FT-IR, SEM, TEM, Raman, etc. These characterizations revealed that ImpGO nanocomposite is comprised of single layer of graphene oxide successfully modified with imprinted polymer. The synthesized material was utilized to selectively determine nicotine using UV-vis spectrophotometer in BR buffer of 0.1 M at pH 3 and diluted human plasma. The effect of parameters such as buffer concentration, pH, amount of nanocomposite, etc on determination of nicotine using ImpGO nanocomposite were studied thoroughly. Thus, a sensitive optical method was developed for determination of nicotine in human plasma with linear range of 22-370 pM along with LOD and LOQ of 7 pM and 22 pM, respectively. The selectivity of sensor was evaluated using homologues of nicotine such as nicotine amide, caffeine and cotinine. The results obtained from biological samples showed that developed optical sensor is efficient in complex matrices of real sample.

Key words: Graphene oxide, Imprinting, Nanocomposite, Nicotine, Selectivity, Optical sensing.

Introduction

Nicotine, 3-(1-methyl-2-pyrolidinyl) pyridine is a hygroscopic oily liquid present in the leaves of Nicotiana tabacum. It is one of the highly toxic chemicals belonging to the tobacco alkaloids [1]. A tobacco plant contains 5 percent nicotine by weight. Cigarettes contain 8 to 20 milligrams (mg) of nicotine (depending on the brand), but only approximately 1 mg is absorbed in the human body. The deep inhalation of cigarette smoke carries nicotine to the central nervous system within 20s. Nicotine affects nicotinic cholinergic receptors and most organ systems in the body because it is one of the highly addictive drugs [2]. The prominent symptoms of exposure to nicotine are bronchitis, emphysema, cyanosis, etc. Therefore, excessive smoking causes lung cancer, bladder cancer, and cancer of the larynx and esophagus [3]. Nicotine also affects appetite and food intake [4]. The above mentioned drawbacks urge to determine trace level of nicotine using highly selective analytical methods. The analytical methods based on sensing phenomenon are replacing conventional analytical methods based on tedious extraction protocols and expensive instruments. This is due to the high selectivity and sensitivity of sensing materials that are the heart of sensor. The selectivity of graphene based optical sensors can be enhanced efficiently by making composites with molecular imprinted polymers. Molecularly imprinted polymers are synthesized in the presence of template molecule by using molecular imprinting technique, after the removal of template, the specific binding sites with same shape, size and orientation of functionalities are left into the polymeric matrix. These imprinted binding sites have an affinity for the template molecule over other structural related compounds [5]. MIPs offer several advantages such as high selectivity, recognition properties, reproducibility robustness, stability, low cost, and ease of scale preparation which are very useful for the development of high performance sensor [6, 7]. The graphene oxide (GO) based molecularly imprinted polymers exhibit excellent affinity and selectivity for target molecule. Like graphene, graphene oxide has high rebinding capacity, large surface area that helps in complete removal of templates. The accessibility and kinetics of target molecules have been improved by graphene oxide due to large surface area which helps template molecule to be on its surface. The combination of GO and molecularly imprinted polymers leads to greater sensitivity and affinity for detection of molecule of interest [8] because sensitivity of detection of an imprinted sensor depends on specific imprinted sites on the surface of the sensor and use of composite materials [5]. Moreover, imprinted GO composite materials in sensors have received increased attention because of their remarkable properties, large surface area, ultra fast response time, excellent biocompatibility, high surface to volume ratio, broad band light absorption, ability to quench florescence, outstanding robustness and flexibility [9]. They are material with stability, high mechanical strength and fascinating electronic and optical properties. Graphene oxide is considered to

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enhance nano electronics for swift optical communications due to its excellent optical behaviors [10]. These properties of graphene oxide are excellent for using them as detection material and can also give very sensitive spectroelectrochemical methods based on it have high detection and quantification limits. However, graphene oxide based composites can perform as sensitive optical sensors very well even for visible spectrophotometer. Wang et al. [11] have developed visible light photoelectrochemical sensor for the detection of 4-aminophenol. The developed sensor was based on MIP/CdS-GR/FTO modified electrode. The photoelectrochemical response was linear in the range of 5.0×10⁻⁸ mol/L to 3.5×10⁻⁶ mol/L and detection limit was found to be 2.3×10⁻⁹ mol L⁻¹. Li et al. [12] have developed sensor for electrochemical detection of dibutyl phthalate. The developed sensor was based on (MGO@AuNPs-MIPs). The response was linear in the range from 2.5×10⁻⁹ to 5.0×10⁻⁶ mol/L with a detection limit of 8.0×10⁻¹⁰ mol/L. Zeng et al. [13] have also developed sensor for electrochemical detection of 4-nitrophenol. The proposed sensor was comprised of rGO and MIP composites. The sensor response was linear from 0.001 to 100.0 μM with limit of detection of 0.005 μM. Cui et al. [14] have reported molecularly imprinted sensor based on PtAu-GrCNTs composite for the detection of propyl gallate. Under optimal condition the sensor response was linear from 7×10⁻⁸ to 1×10⁻⁵ mol L⁻¹ of propyl gallate with limit of detection of 2.51×10⁻⁸ mol L⁻¹. Luo et al. [15] have developed electrochemical sensor for the detection of 4-nitrophenol. The developed sensor was based on GR/MIPs composite. The response of sensor was linear in range 0.01 to 100 μM with a limit of detection 5 nM. Yao et al. [16] have devised SPR sensor for the detection of ractopamine. The developed sensor was comprised of MIP/GNPs/rGO composite. The sensor response was linear from 20 ng/mL to 1000 ng/mL with a detection limit of 5 ng/mL. Bagheri et al. [17] have proposed sensor for electrochemical detection of nitrite and nitrate. The developed sensor is based on (Cu/MWCNT/RGO). The sensor response was linear from 0.1 μM to 75 μM with detection limits 30 nM and 20 nM. More recently, Zhang et al. [18] prepared sensor based on CdTe@[emim]MP-aminRGO nanocomposite for electrochemical detection of puerarin. Similarly, Gao et al. [19] developed sensor comprised of HAP-rGO nanocomposite for electrochemical detection of hydrazine. The sensor responded linear in the range of 2.5 μM to 0.26 mM with a limit of detection of 0.43 μM. Er et al. [20] synthesized sensor based on PtNPs@GRP/NFN/GCE nanocomposite for electrochemical detection of Silidosin. The sensor response was linear from 1.8 nM to 290.0 nM with limit of detection 0.55 nM. Thus, most of the recently reported sensors based on graphene or graphene oxide nanocomposites are electrochemical sensors with fewer reports of SPR sensors. The SPR based sensing technique is comparatively more expensive among the other optical sensing techniques. Moreover, the reports for sensitive UV-vis spectrophotometer based graphene/graphene oxide nanocomposites optical sensors are even less.

In this work, we have developed novel Nicotine imprinted graphene oxide nanocomposite (ImpGO nanocomposites) and utilized it for optical sensing based on ultra sensitive UV-visible spectrophotometric detection of nicotine in human plasma. UV-vis spectrophotometer is relatively cheaper, swift and simple technique as compared to other optical devices. Imprinted graphene oxide composite provided specific binding sites for nicotine. The developed optical sensor exhibited an excellent selectivity and sensitivity for the detection of nicotine down to pM. Based on obtained results, the proposed optical sensor comprised of imprinted graphene oxide composite was effectively used to detect nicotine in human blood plasma.

**Experimental**

The details of chemicals and reagents is given in the supplementary data under section 2.1.S

The details of instrumentation is also given in the supplementary data under section 2.2.S

**Synthesis of nicotine ImpGO nanocomposite**

GO was synthesized using graphite flakes by Hummer’s method [21]. Synthesized GO was intercalated with thiosalicylic acid (TSA) (10%). Precisely, 4 mL of thiosalicylic acid (10%) and 20 mg GO were added in a beaker and heated at 80 °C for 4 hours in hot water bath. Here heating is necessary to unstack and straighten the stacked sheets of GO. Resulting product was then allowed to cool down and washed thoroughly with deionized water to remove excess of TSA. To prepare imprinted nano-composite; first prepolymerization complexation was carried out by dissolving 0.1 M nicotine standard (template) in 16 mL of DI water maintained at pH 3. To this solution 10 mg of TSA intercalated GO (TSA@GO) was added and mixture was sonicated for 2 hours. Then to this mixture; 2 mL of pyrrole was added and stirred at 95 °C for 12 hrs. The prepared material was washed by methanol for removal of nicotine. Fig. 1 shows the schematic representation of synthesis procedure for ImpGO nanocomposite.
Fig. 1: Schematic representation for the synthesis of Nicotine imprinted GO nanocomposite.

The procedures for optimization of optical parameters for detection of nicotine using ImpGO nanocomposites, evaluation of selectivity of developed sensor and collection and processing of real samples are given in supplementary data under sections 2.3.S, 2.4.S and 2.5.S, respectively.

**Result and Discussion**

**Characterization**

The detailed FTIR spectra and their explanation is given in the supplementary data under section 3.1.S

Raman spectroscopy is technique that is often used to study the defects disorders and layers of graphene oxide. There are two main features of Raman spectra that characterize graphene oxide. The G-mode that appears in first order scattering E2g photon of sp² carbon atoms appear at higher energy 1575 cm⁻¹ while breathing mode within A1g symmetry of j-point arising from D band appearing at lower energy i.e. 1350 cm⁻¹. In Fig 2A which is the raman spectra of GO the G band appears around 1587 cm⁻¹ because of the existence of isolated double bonds that vibrate at higher frequencies. Increased prominence in the D band at 1314 cm⁻¹ shows layer thickness increases i.e. bilayer of graphene oxide is present [23]. The D band is also known as disorder or defect band and its intensity indicates the level of defect in graphene oxide. Conversely, in TSA@GO after intercalation its intensity decreased which indicates that the defect has been reduced. In (Fig 2B) the D/G intensity ratio for TSA@GO is 1.1 which is lower than GO i.e. 1.4 indicates that TSA has been intercalated with GO [24]. In (Fig 2C) the G band at 1658 cm⁻¹ comes from polypyrrole this peak combined with G band to give broad G band [25]. Conversely, the D/G ratio decreases to 0.5 because of decrease in disorder of synthesized material. 2D peak is important in the Raman spectroscopy. Its position and shape are used to predict number of graphene oxide layers. 2D peak is appearing lower than 2700 cm⁻¹ indicating the presence of single layer of graphene oxide. If it appears at 2700 cm⁻¹, then the bilayer graphene oxide is present. In (Fig 2C) ImpGO nanocomposite the 2D peak at around 2099 cm⁻¹ indicates that single layer of graphene is present in this composite [26].

SEM study is used to investigate the surface morphology of ImpGO nanocomposite. In (Fig 3A) graphite shows stacked sheets. However, the surface morphology of GO has been changed as shown in (Fig 3B) [27]. In comparison to GO, TSA@GO (Fig 3C) exhibits a curved thin flaky appearance. In (Fig 3D) ImpGO nanocomposite shows a dense and quite rough surface, indicating that imprinted polypyrrole has aligned on the surface of ImpGO nanocomposite [15].
Fig. 2: Raman spectra of (A) GO, (B) TSA@GO, (C) ImpGO nanocomposite.
The morphological structure of prepared material was also examined by TEM. In Fig 4A, the wrinkles on GO show sheet like morphology is preserved while the darker portion shows more graphene sheets [28]. While in (Fig 4B) TSA@GO wrinkles are retained even after intercalation but the number of stacked sheets has been reduced after intercalation [24]. Whereas, the (Fig 4C) TEM image of ImpGO nanocomposite shows that one sheet is being aligned with the nicotine imprinted polypyrrole. However, wrinkles are still there and sheet is uniformly distributed with nicotine imprinted polypyrrole [29].

Interaction of ImpGO nanocomposite with nicotine

Fig 5 shows Uv-visible spectra of ImpGO nanocomposite in the presence of nicotine (22 pM) and ImpGO nanocomposite alone in water. It is clearly seen that ImpGO nanocomposite does not show any absorption around 295 nm. However, when minute concentration of nicotine is added a band appeared at 295 nm due to the presence of nicotine. Moreover, the characteristic peak of nicotine around 260 nm shifted to 295 nm which is a red shift occurred due the interaction of ImpGO nanocomposites with nicotine. Uv-vis spectrophotometer cannot detect such low concentration of nicotine in the absence of sensing material; it is due to the incorporation of graphene oxide and MIP which resulted in composite material that provides a sensitivity enhancement by inducing large field enhancement at the substrate interface [30]. Furthermore, imprinting is also playing its role in selectivity of sensing material as ImpGO nanocomposite contains imprinted binding sites which recognize the nicotine selectively and get activated.

Optimization of amount of ImpGO nanocomposite

To optimize the amount of ImpGO nanocomposite for maximum response of nicotine, the standard solution of nicotine (7 pM) was spiked with different amounts of ImpGO nanocomposite. As observed in (Fig 3S) when the amount of ImpGO nanocomposite increases from 10 µg to 220 µg in 7 pM of nicotine the response greatly enhances till 200 µg of ImpGO nanocomposites, however, slight increments occurrence with further increase of the ImpGO nanocomposite. Thus, 200 µg of ImpGO nanocomposite was selected for further studies [31]. The Uv-visible
spectra of effect of amount of ImpGO nanocomposite for the maximum response of nicotine is given in the supplementary data in Fig 3.S.

**Optimization of pH and buffer concentration**

The pH was investigated using 0.1 M Britton-Robinson Buffer in the range of pH 2 to 12 and response of 7 pM of nicotine was checked on ImpGO nanocomposite. It was observed that (Fig 6) at 295 nm ImpGO nanocomposite showed maximum response with BR buffer of pH 3. The maximum intensity and exact position of peak depends upon nature of solvent, analyte and sensing material [32]. Depending on pH the nicotine may be found in one of three types such as mono protonated, diprotonated and unprotonated [33]. It is mono protonated at pH less than 3, diprotonated at pH 3 to 8 and unprotonated at pH greater than 8, respectively [34]. Nicotine is basic compound having two pKa values of 8.02 and 3.12 and having capability to form hydrogen bonds [35]. Thus, keeping this in mind the pre-polymerization complexation of nicotine with TSA@GO was carried out at pH 3. Therefore, it interacts with ImpGO nanocomposite through hydrogen bonds at pH 3 as the active binding sites are selective to diprotonated nicotine. However, the absorption band shifts from 260 nm to 295 nm due to interaction of nicotine with ImpGO [36]. Therefore, BR buffer at pH 3 was selected for further studies.

![Fig 5: The UV-visible spectra of interaction; Insight (A) ImpGO nanocomposite, (B) ImpGO nanocomposite with nicotine.](https://example.com/fig5)

![Fig. 6: Effect of BR buffer at different pH on sensing efficiency of ImpGO nanocomposite for nicotine.](https://example.com/fig6)
Fig 4S in supplementary data shows the influence of buffer concentration on sensing ability of ImpGO nanocomposite for nicotine. The BR buffer of pH 3 was evaluated in the concentration range of 0.005 to 0.5 M. It is clearly seen that with the increase in concentration of BR buffer the response of ImpGO nanocomposite linearly increases till 0.1 M (peak at 295 nm) due to the interaction of nicotine with the ImpGO nanocomposite. Conversely, further increase in concentration of BR buffer decreased the response. This may be due to the influence of higher concentration of buffer components that inactivate the binding sites. Therefore 0.1M BR buffer of pH 3 was selected for further studies.

Table 1: Analytical Figs of merit for determination of nicotine using ImpGO nanocomposite in human plasma

<table>
<thead>
<tr>
<th>Analytical Figs of Merit</th>
<th>Linear Range (pM)</th>
<th>Linearity ($r^2$)</th>
<th>Slope (a)</th>
<th>Intercept (b)</th>
<th>LOD (pM)</th>
<th>LOQ (pM)</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>22-370</td>
<td>0.999</td>
<td>0.00026</td>
<td>0.24</td>
<td>7</td>
<td>22</td>
</tr>
<tr>
<td>Intra-assay Precision (RSD %)</td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>22 pM (n=3)</td>
<td>0.86 %</td>
<td>0.74 %</td>
<td>0.16 %</td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Inter-assay Precision (RSD %)</td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>22 pM (n=3, 3days)</td>
<td>0.76 %</td>
<td>0.68 %</td>
<td>0.14 %</td>
<td></td>
<td></td>
<td></td>
</tr>
</tbody>
</table>

In order to check the effect of complex matrices on the performance of ImpGO nanocomposite, a method was also developed and validated in blood plasma using ImpGO nanocomposite. The human blood plasma was processed, spiked with different concentrations of nicotine and diluted with 0.1 M BR buffer as described in section 2.4S in supplementary data. The Table 1 shows the analytical Figs of merit for determination of nicotine in blood plasma. In this method the linear range was obtained from 22 to 370 pM with the linearity 0.999 whereas the limit of detection 7 pM and limit of quantification 22 pM were obtained with acceptable RSD values of intraday and interday precision (Fig 7). The results clearly show that the efficiency of ImpGO nanocomposite is not compromised even in complex matrices. However, the absorption peak of nicotine is observed at around 275 nm. This shift of absorption band from 295 nm (BR Buffer) to 275 nm (diluted plasma) in the presence of ImpGO composites is due to the matrix effect. The excellent LOD and LOQ values show that in spite of complex matrix the selectivity and sensitivity of sensing material is not compromised. The sensitivity and specificity of ImpGO nanocomposite for nicotine in blood plasma is almost same as it was in the standard solutions of nicotine.

Interference study

The imprinting factor is used to determine the selectivity of prepared imprinted material; it shows the strength of interaction of template and functional monomer. If the imprinting factor value is greater, it indicates that there is strong interaction between template and functional monomer. If the imprinting factor value is smaller, it indicates that there is weak interaction between template and functional monomer [37]. The imprinting factor of nicotine imprinted graphene oxide nanocomposite was checked with the homologues of nicotine such as nicotinamide, caffeine and cotinine in human plasma. The imprinting factor was calculated using following equation by taking the absorbance of nicotine and its homologues having same concentration, using imprinted and non-imprinted graphene oxide nanocomposite.

Coefficient of selectivity ($k_i$) = \frac{Abs (template)}{Abs (competitor)}

Relative Selectivity Coefficient ($k'$) = \frac{k (ImpGO nanocomposite)}{k (ImpGO nanocomposite)}

The selectivity study (Table 2) revealed that nicotine imprinted graphene oxide nanocomposite is 2.4 times more selective for nicotine than nicotinamide and 1.6 times more selective for nicotine than caffeine and 1.1 times more selective for nicotine than cotinine due to specific binding sites that recognize the target molecule.

Recovery study

The developed method was applied on real samples such as blood plasma of smokers. In this regard the three different concentration of nicotine were spiked in blood plasma of smokers along with ImpGO nanocomposite. The Table 3 shows the recoveries % obtained from blood plasma of smokers. In all samples, there is negligible matrix effect as the prepared material is more selective and sensitive for nicotine.
Table-2: Selectivity and relative selective coefficient of ImpGO nanocomposite.

<table>
<thead>
<tr>
<th>Alkaloids</th>
<th>ImpGO nanocomposite</th>
<th>NImpGO nanocomposite</th>
<th>k</th>
<th>ImpGO nanocomposite</th>
<th>k</th>
<th>NImpGO nanocomposite</th>
<th>k'</th>
</tr>
</thead>
<tbody>
<tr>
<td>Nicotine</td>
<td>0.34</td>
<td>0.14</td>
<td></td>
<td>3.7</td>
<td>1.5</td>
<td>2.4</td>
<td></td>
</tr>
<tr>
<td>Nicotine amide</td>
<td>0.09</td>
<td>0.09</td>
<td></td>
<td>2.8</td>
<td>1.75</td>
<td>1.6</td>
<td></td>
</tr>
<tr>
<td>Caffeine</td>
<td>0.12</td>
<td>0.08</td>
<td></td>
<td>1.9</td>
<td>1.7</td>
<td>1.1</td>
<td></td>
</tr>
<tr>
<td>Cotinine</td>
<td>0.18</td>
<td>0.08</td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
</tbody>
</table>

Table-3: Recovery % of spiked human plasma using ImpGO nanocomposite for nicotine.

<table>
<thead>
<tr>
<th>Conc.(pM)</th>
<th>Recovery %</th>
</tr>
</thead>
<tbody>
<tr>
<td>Nicotine</td>
<td>Plasma 1</td>
</tr>
<tr>
<td>22</td>
<td>90</td>
</tr>
<tr>
<td>155</td>
<td>93</td>
</tr>
<tr>
<td>370</td>
<td>97</td>
</tr>
</tbody>
</table>

Conclusion

A new optically active nicotine imprinted graphene oxide nanocomposite was prepared. The nanocomposite was utilized for selective optical sensing of nicotine in human blood plasma. The calibration curve for nicotine determination was obtained at optimized conditions using human blood plasma diluted with 0.1 M BR buffer at pH 3. Linear range and limit of detection at ultra trace levels of nicotine (pM) were obtained. Furthermore, short analysis time, good selectivity and accuracy, low cost and simple preparation process are among the advantages of the proposed sensor. The proposed nanocomposite is excellent for sensing of nicotine in biological samples.

Conflict of interest

All the authors of this manuscript declare that there are no conflicts of interest to declare for the research data presented in this manuscript.
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